## VIBE

Visualization of Intrafraction Behavior from Electromagnetic Tracking

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## Presentation Overview

- Define the problem \& medical background
- Identify goals of the project
- Outline my process
- Demo the final animation
- Discuss medical contributions
- Suggest future directions


## Problem Definition

- Organs naturally move during the course of radiation treatments
- Sidenote: Intrafraction motion = organ movement within one treatment on a given day
- Interfraction motion = organ movement between treatments on different days
- Though more obvious in organs like the lungs, which expand and contract with breathing, other organs, like the prostate, also demonstrate movement
- Radiation that reaches non-target (non-cancerous) tissue may result in various side effects
- There has been an effort in radiation therapy to improve the precision of cancer treatments, reducing side effects and better controlling tumors


## Background

- Accuracy of radiation is challenging due to natural organ movement during treatments
- Radiology Oncologists are working to improve the precision of cancer treatments - to better target tumor-bearing tissue and to reduce the unintentional doses reaching normal tissue - by tracking the motion and deformation of the cancerous organ
- The Calypso® 4D Localization System uses electromagnetic sensors to track the exact position and motion of the organ in real-time
- For this, it is sometimes described as "GPS for the Body®"


## How does Calypso ${ }^{\circledR}$ work?

- Prior to treatment, three Beacon® transponders are implanted into the target tissue, in this case, the prostate gland


Beacon® ${ }^{\circledR}$ transponder ( 8 mm in length)

- Beacon ${ }^{\circledR}$ transponders are tiny electromagnetic sensors, which monitor the position and motion of the organ
- Through safe radiofrequency waves, the Calypso System tracks and records the location of each transponder
- Can be thought of as "motion capture for organs"



## Project Goals

- Understand intrafraction prostate motion by visualizing and reanimating organ contours
- Provide results for Radiology Oncologists, allowing them to interpret the outcomes and determine their practical application and significance
- Presenting data with which to identify potential motion patterns


## Tools \& Languages

- Calypso 4D Localization System
- Beacon® Transponders
- MATLAB
- Excel (VBA)


## Resampling the Data

- The Calypso machine records and outputs the location of each transponder sequentially so the original excel document looks like the following:

| Transponder | $\mathbf{X}$ | $\mathbf{Y}$ | $\mathbf{Z}$ | PositionTimeString |
| ---: | :---: | :---: | :---: | :---: |
| 1 | 0.768007685 | -0.670575507 | 1.237602205 | 2008-02-12T15:14:24.9445000-05:00 |
| 2 | 0.543598218 | 0.305644489 | -1.031243917 | $2008-02-12 \mathrm{~T} 15: 14: 25.0355000-05: 00$ |
| 3 | -1.595396957 | 0.522831979 | -0.420960678 | $2008-02-12 \mathrm{~T} 15: 14: 25.1165000-05: 00$ |
| 1 | 0.773501245 | -0.685332166 | 1.253303285 | $2008-02-12 \mathrm{~T} 15: 14: 25.2385000-05: 00$ |
| 2 | 0.530271027 | 0.278862085 | -1.017448201 | $2008-02-12 \mathrm{~T} 15: 14: 25.3195000-05: 00$ |
| 3 | -1.606955031 | 0.507740164 | -0.432733083 | $2008-02-12 \mathrm{~T} 15: 14: 25.4005000-05: 00$ |

- Want location of transponders at the same instance to track movement and deformation of three-transponder triangle over a period of time
- In order to obtain this triangle, the data must be resampled


## Resampling the Data

- Generate b-spline curves to explain the position and movement of each transponder independently in order to retrieve its position at any time during the 18 minute interval
- Using VBA code, create separate sheets that isolate each transponder's $\mathrm{x}, \mathrm{y}, \mathrm{z}$ position, like so:

| Transponder | $\mathbf{X}$ | $\mathbf{Y}$ | $\mathbf{Z}$ | PositionTimeString |
| ---: | :---: | :---: | :---: | :---: |
| 1 | 0.768007685 | -0.670575507 | 1.237602205 | $2008-02-12 T 15: 14: 24.9445000-05: 00$ |
| 1 | 0.773501245 | -0.685332166 | 1.253303285 | $2008-02-12 T 15: 14: 25.2385000-05: 00$ |
| 1 | 0.765768046 | -0.703897066 | 1.261517722 | $2008-02-12 T 15: 14: 25.5525000-05: 00$ |
| 1 | 0.770603624 | -0.703192297 | 1.257850022 | $2008-02-12 T 15: 14: 25.8365000-05: 00$ |
| 1 | 0.771952138 | -0.705367329 | 1.250430385 | 2008-02-12T15:14:26.1505000-05:00 |

- Format allows me to copy an entire column (about 3650 times) into an array and graph the movement along one of the axes over time


## Resampling the Data

- Convert timestamps from 2008.02:1211/5:1424.4945000.05:00 to seconds using another VBA parsing function
- Remove spurious data (specifically zeros, where the machine might have faulted)
- Ready to graph


## Resulting Graphs

$\Theta 00 \quad$ <Student Version> Figure 1 File Edit View Insert Tools Desktop Window Help



QOO <Student Version> Figure 2 File Edit View Insert Tools Desktop Window Help


$\Theta 00 \quad$ <Student Version> Figure 3 File Edit View Insert Tools Desktop Window Help



- X, Y, and Z position graphs for Transponder 1 demonstrate some shift around 500 seconds
- $\quad$ Similar graphs are generated for T2 and T3 (9 total)


## Resulting Graphs





- Transponder 1 b-spline curves, which can later be interpolated from to find positions at any time


## Interpolation

- Interpolate from each of the 9 graphs to obtain the three-dimensional locations of each transponder at every second, generating three points to create a triangle

| T1 |  |  | T2 |  |  | T3 |  |  |
| :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: |
| x | y | Z | x | y | z | x | y | z |
| 0.7677 | -0.6713 | 1.2385 ; | 0.5427 | 0.3005 | -1.0336; | -1.6027 | 0.5202 | -0.4254; |
| 0.7625 | -0.6838 | 1.2551 ; | 0.5427 | 0.3005 | -1.0336; | -1.6027 | 0.5202 | -0.4254; |
| 0.7623 | -0.6899 | 1.2590 ; | 0.5409 | 0.2947 | -1.0305; | -1.6073 | 0.5170 | -0.4247; |
| 0.7669 | -0.6938 | 1.2542 ; | 0.5382 | 0.2886 | -1.0218; | -1.6066 | 0.5136 | -0.4160; |
| 0.7857 | -0.7359 | 1.2553 ; | 0.5484 | 0.2296 | -1.0264; | -1.5884 | 0.4618 | -0.4088; |
| 0.7824 | -0.7274 | 1.2477 ; | 0.5505 | 0.2276 | -1.0324; | -1.5750 | 0.4530 | -0.4146; |
| 0.7660 | -0.6884 | 1.2363 ; | 0.5445 | 0.2795 | -1.0389; | -1.5701 | 0.5065 | -0.4369; |
| 0.7635 | -0.6767 | 1.2409 ; | 0.5350 | 0.3304 | -1.0342; | -1.5994 | 0.5270 | -0.4460; |
| 0.7610 | -0.6877 | 1.2461 ; | 0.5269 | 0.3151 | -1.0342; | -1.6127 | 0.5200 | -0.4471; |
| 0.7586 | -0.7098 | 1.2502 ; | 0.5199 | 0.2539 | -1.0372; | -1.6070 | 0.4856 | -0.4406; |
| 0.7579 | -0.7243 | 1.2456 ; | 0.5131 | 0.2594 | -1.0337; | -1.6037 | 0.4787 | -0.4362; |
| 0.7578 | -0.7055 | 1.2492 ; | 0.5193 | 0.2828 | -1.0385; | -1.6053 | 0.4977 | -0.4388; |
| 0.7581 | -0.6752 | 1.2542 ; | 0.5338 | 0.3153 | -1.0473; | -1.6117 | 0.5411 | -0.4481; |
| 0.7594 | -0.6686 | 1.2465 ; | 0.5388 | 0.3118 | -1.0380; | -1.6074 | 0.5301 | -0.4453; |
| 0.7765 | -0.6923 | 1.2463 ; | 0.5399 | 0.2912 | -1.0419; | -1.6055 | 0.5122 | -0.4496; |
| 0.7906 | -0.7162 | 1.2451 ; | 0.5380 | 0.2669 | -1.0523; | -1.6057 | 0.4897 | -0.4599; |
| 0.7664 | -0.6899 | 1.2273 ; | 0.5321 | 0.2940 | -1.0499; | -1.6040 | 0.5033 | -0.4703; |

## Filtering Data

- Because the accuracy of the machine is .1 mm , much of the perceived movement is machine noise
- Format excel columns to display only 1 decimal place

| T1 |  |  | T2 |  |  | T3 |  |  |
| :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: |
| x | y | z | x | y | z | x | y | z |
| 0.8 | -0.7 | 1.2 ; | 0.5 | 0.3 | -1.0; | -1.6 | 0.5 | -0.4; |
| 0.8 | -0.7 | 1.3 ; | 0.5 | 0.3 | -1.0; | -1.6 | 0.5 | -0.4; |
| 0.8 | -0.7 | 1.3 ; | 0.5 | 0.3 | -1.0; | -1.6 | 0.5 | -0.4; |
| 0.8 | -0.7 | 1.3 ; | 0.5 | 0.3 | -1.0; | -1.6 | 0.5 | -0.4; |
| 0.8 | -0.7 | 1.3 ; | 0.5 | 0.2 | -1.0; | -1.6 | 0.5 | -0.4; |
| 0.8 | -0.7 | 1.2 ; | 0.6 | 0.2 | -1.0; | -1.6 | 0.5 | -0.4; |
| 0.8 | -0.7 | 1.2 ; | 0.5 | 0.3 | -1.0; | -1.6 | 0.5 | -0.4; |
| 0.8 | -0.7 | 1.2 ; | 0.5 | 0.3 | -1.0; | -1.6 | 0.5 | -0.4; |
| 0.8 | -0.7 | 1.2 ; | 0.5 | 0.3 | -1.0; | -1.6 | 0.5 | -0.4; |
| 0.8 | -0.7 | 1.3 ; | 0.5 | 0.3 | -1.0; | -1.6 | 0.5 | -0.4; |
| 0.8 | -0.7 | 1.2 ; | 0.5 | 0.3 | -1.0; | -1.6 | 0.5 | -0.4; |
| 0.8 | -0.7 | 1.2 ; | 0.5 | 0.3 | -1.0; | -1.6 | 0.5 | -0.4; |
| 0.8 | -0.7 | 1.3 ; | 0.5 | 0.3 | -1.0; | -1.6 | 0.5 | -0.4; |

## Animating Triangle

- With three points in space, can plot triangle
- Calculate mins and maxs and from this, compute bounding box

```
Ffunction box = boundingBox(P1, P2, P3)
    ztriangle vectors
    x=[[P1(1)
    y =[P1(2) P2(2) P3(2)];
    %calculate all 6 mins and maxs
    mins = calcMins(P1, P2, P3);
    minX = mins(1); minY = mins(2); minZ = mins(3);
    maxs = calcMaxs(P1, P2, P3); ; ; maxZ = maxs(3);
    *square vectors
    xbox1 = [minX maxx maxx minX minX]
    ybox1 =[minY minY minY minY minY];
    ybox1 =[minY minY minY minY minY m;
    ybox2 = [maxY maxY maxY maxY maxY];
    xbox3 = [maxX maxX maxX maxX maxX];
    xbox4 = [minX minX minX minX minX];
    splot all four squares to create cube and plot triangle
    figure(1);
    axis('square');
    fil13(x,y,z,'r');
    hold on (xbox1,ybox1,zbox1,'b',xbox1,ybox2,zbox1,'b',xbox3,ybox3,zbox1,'b',xbox4,ybox3,zbox1,'b');
    plot3(xbo
box = 0;
```

end

## Animating Triangle

- To see the changes over time, I wrote a function called "animate," which creates an .avi file of a sequence of all of the frames

```
function animation = animate(P1, P2, P3)
[length, three] = size(P1);
aviobj=avifile('test2.avi');
hf= figure('visible','off');
for i = 1:length
    p1 = [P1(i,1), P1(i,2), P1(i,3)];
    p2 = [P2(i,1), P2 (i,2), P2 (i,3)];
    p3 = [P3(i,1), P3(i,2), P3(i,3)];
    boundingBox(p1,p2,p3);
    aviobj=addframe(aviobj,hf);
end
*movie(M);
aviobj=close(aviobj);
end
```



## Finding Transformation Matrices

- First plot graphs for 1) Centroid movement in the X, Y, and Z directions, 2) Rotation between each frame and the first, and 3) scale change in each direction
- Because the scale change is mainly constant in all dimensions, Dr. Badler and I chose only to consider translation and rotation


Centroid Movement


Rotation

## Finding Transformation Matrices

- Next step: for each triangle, compute 1) translation and 2) rotation matrix between first and current frame
- Use tMatrices, rMatrices functions to output an array of matrices for each frame, which can then be applied in a for-loop to animate the contour


## Finding Transformation

## Matrices

```
function matrices = rMatrices(P1, P2, P3)
[length, three] = size(P1);
matrices = zeros(4,4,length-1);
normals = calcNormals(P1, P2, P3);
angles = plotAngles(P1, P2, P3);
centroid = calcCentroids(P1, P2, P3);
for i = 1:length-1
    v1 = [normals(i,1) normals(i,2) normals(i,3)];
    v2 = [normals(i+1,1) normals(i+1,2) normals(i+1,3)];
    %find rotation axis by taking cross product of consecutive frames
    *normals
    w = cross(v1, v2);
    wLength = sqrt(w(1)^2 + w(2)^2 + w(3)^2)
    if wLength ~= 0
    w = w/wLength;
    W end
    a=w(1);
    c=w(3)
    theta = angles(i)
    %use values from the rotation axis vector ( }\textrm{w}=[\textrm{a},\textrm{b},\textrm{c}])\mathrm{ ) and the angle
    *between the two normals to plug into rotation matrix; combine values
    %for translation
    m}=[\mp@subsup{a}{}{\wedge}2+(1-\mp@subsup{a}{}{\wedge}2)**\operatorname{cos}(theta), a*b*(1-cos(theta))-c*sin(theta), a*c*(1-cos(theta))+b*sin(theta), 0;
        a*b*(1-cos(theta))+c*sin(theta), b^2+(1-b^2)**os(theta), b*cc*(1-cos(theta))-a*sin(theta), 0;
        a*c*(1-cos(theta))-b*sin(theta), b* c*(1-cos(theta))+a*sin(theta), c^2+(1-c^2)*\operatorname{cos(theta),, 0;}
        0, 0, 0, 1];
    matrices(:,:,i) =m;

\section*{Displaying Contours}

Data provided:
\begin{tabular}{ccc}
\(X\) & \(Y\) & \(Z\) \\
-10.205 & -295.748 & 164.664 \\
-8.057 & -295.761 & 164.664 \\
-5.908 & -295.569 & 164.664 \\
-3.959 & -295.221 & 164.664 \\
-3.76 & -295.179 & 164.664 \\
-1.611 & -294.674 & 164.664 \\
0.537 & -294.105 & 164.664 \\
2.686 & -293.528 & 164.664 \\
4.441 & -293.072 & 164.664
\end{tabular}
- Each row represents a point along one contour loop, and each loop is separated by a blank row
- MATLAB does not recognize blank rows, so I replaced blanks with an indicator (arbitrarily 5000000) so that a function could recognize the end of a contour loop
- Before animating, I tested the 3-D contour display with the function drawContour

\section*{Displaying Contours}
drawContour generates a 3-D wireframe of the prostate, which can be rotated in MATLAB to display different perspectives

function contour \(=\) drawContours \((X, Y, Z)\)
[length, one] = size(X);
temp \(=0\);
firstX \(=\mathrm{X}(1)\);
firsty \(=\mathrm{Y}(1)\);
firstz \(=Z(1)\);
*make each contour line form a full circle sby filling in the blank with the first
selement of the loop
for \(i=1\) length
if \(X(i)=5000000\)
\(\mathrm{X}(\mathrm{i})=\mathrm{firstx}\)
\(Y(i)=\) firsty;
\(\mathrm{Z}(\mathrm{i})=\mathrm{firstz}\);
if i ~= length
firstX \(=\mathrm{X}(\mathrm{i}+1)\);
firsty \(=\mathrm{Y}(\mathrm{i}+1)\);
firstz \(=Z(i+1)\);
end
sdraw the contour lines
for \(j=1: i\)-temp
\(a(j)=x(j+\) temp \() ;\)
\(b(j)=Y(j+\) temp \() ;\)
\(c(j)=z(j+\) temp \() ;\)

\section*{end}
plot3(a,b, c) ;
hold on;
temp \(=i ;\)
end
end
hold off; end

\section*{Animating Contours}
- Ran into several problems
- "Frozen screen" effect because of overriding initial array that contains indicators
- Correctly displaying wireframe and holding axes constant
- Jumping around - incorrect rotation matrix

\section*{Animating Contours}
for \(i=1\) :time- 1
irstX \(=\) origx (1);
firstz \(=\) origy (1);
\(m=\operatorname{tm}(:,:, i) \star r m(:,:, i) * \operatorname{tim}(:,:, i)\);
for \(\begin{aligned} & j=1: \text { numpoints } \\ & \text { if } \operatorname{orig}(j)= \\ & x=5000000\end{aligned}\)
\(x(j)=\) firstx;
\(Y(j)=f i r s t y ;\)
\(\underset{\text { if }}{\mathrm{Z}}(\mathrm{j})=\) firstz \(;=\) numpoint

firsty \(=\operatorname{origy}(j+1) ;\)
firstZ \(=\operatorname{origZ}(j+1) ;\)
end
smultiply by matrix
newX \((j)=m(1,1) * X(j)+m(1,2) * Y(j)+m(1,3) * Z(j)+m(1,4) ;\) newY \((j)=m(2,1) * X(j)+m(2,2) \star Y(j)+m(2,3) \star Z(j)+m(2,4) ;\)
newZ \((j)=m(3,1) * X(j)+m(3,2) * Y(j)+m(3,3) * Z(j)+m(3,4) ;\)
odraw the contour lines
for \(k=1: j\)-temp
XLOOp (k) \(=\) newX ( \(k+\) temp );
zLoop \((k)=\) newZ \((k+\) temp \()\)
end
axis([-100 \(50-350-180110240]) ;\)
plot3(xLoop, yLoop, zLoop):
plot3 (xLoop, yLoop, zLoop) ;
clear xL
temp \(=j\)
else
कmultiply by matrix
newX \((j)=m(1,1) * X(j)+m(1,2) * Y(j)+m(1,3) * Z(j)+m(1,4)\); newY \((j)=m(2,1) * X(j)+m(2,2) * Y(j)+m(2,3) * Z(j)+m(2,4) ;\)
newZ \((j)=m(3,1) * X(j)+m(3,2) * Y(j)+m(3,3) * Z(j)+m(3,4)\) end \({ }^{\text {n }}\)
end
aviobj=addframe(aviobj,hf);

\section*{Issue with Transformation}
- Forced fitting
- Neglecting scale change/deformation
- Causes forced rotation
- Working on computing ONE transformation matrix that takes into account shearing/scaling/compression, in addition to rotation and translation
- Scale disparity
- Small triangle controlling large contour
- Tiny shift in triangle translates into magnified shift in contour

\section*{Issue with Transformation}



\section*{Contributions}
- Ability to visualize organ motion from spaciotemporal data, providing a better understanding of intrafraction prostate motion
- Computing clinically useful measures
- centroid movement, rotation angles, min/max displacement
- Opportunity for identifying patterns of behavior and improving treatment accuracy
- Published in an abstract submitted to ASTRO, the American Society for Therapeutic Radiology and Oncology and another anticipated publication in the near future

\section*{Development of a Novel System for Visualizing Prostate Motion in Patients Undergoing Radiotherapy with Electromagnetic Target Localization and Tracking}

Author Block R. R. Rajendran, T. Nevo, E. Rubin, A. Kassaee, N. Badler, N. Vapiwala
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\section*{Future Directions}
- Fixing "jumpiness" of current animation
- Future application by Radiology Oncologists in effort to reduce error and improve accuracy/effectiveness of therapy
- Ability to import data files and run program directly, essentially reducing number of steps
- Build an interface that displays useful outcomes
- Real-time animation and ultimately automated target monitoring and radiation beam adjustment during treatment

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